

# The Influence of Braiding Angle Variation in Braided-Twisted Fiber Scaffold Based Poly L- Lactic Acid for Anterior Cruciate Ligament Reconstruction Application

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**Submission date:** 13-May-2019 04:03PM (UTC+0800)

**Submission ID:** 1129595773

**File name:** C02\_ACL\_2013.pdf (268.63K)

**Word count:** 2241

**Character count:** 12025

## The Influence of Braiding Angle Variation in Braided-Twisted Fiber Scaffold Based Poly L-Lactic Acid for Anterior Cruciate Ligament Reconstruction Application

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**Keywords:** PLLA; Electrospinning; ACL; Scaffold.

**Abstract.** Anterior Cruciate Ligament (ACL) injury may cause other tissue injuries and degenerative joint diseases, rendering major surgery compulsory. The ACL substitutions from patient's other tissue (autograft), from cadaver (allograft), or from other species (xenograft) still cause problems like donor morbidity, reduction of mechanical strength in cryopreservation period, and the risk of transgenic infection. Tissue engineering approach is the proposed solution. For this, synthetic ligament scaffold is needed. Electrospinning is a method to produce porous scaffolds made of polymers. In this study, filaments were produced from electrospinning poly l-lactic acid. The filaments were then twisted with 60° angle to the horizontal to make a yarn. Subsequently, the yarns were braided with the variation of braiding angle 40°, 60° and 80°. The characterization on the scaffold includes degradation rate, porosity, tensile strength, and cytotoxicity. It was found that larger braiding angle gave higher degradation rate, bigger pore size, and lower mechanical strength. For cytotoxicity, in terms of pore size and percentage of living cell, scaffold with braiding angle of 80° also showed the optimum result.

### Introduction

The Anterior Cruciate Ligament (ACL) is a tissue in knee joint which connects tibia (lower leg) to the femur (thigh). In America, more than 250.000 patients are diagnosed to suffer from ACL torn every year and around 150.000 ACL surgeries are conducted every year. ACL torn is a significant joint injury. It causes other tissue injuries and degenerative joint diseases. The low capacity of ACL torn healing caused orthopedic chooses surgery total reconstruction to the patients. In the clinical practice, there are several options, including autograft, allograft, and xenograft. Autograft is a ligament substitute from the other tissues of the patients. It can be taken from patellar, quadriceps, and hamstring. However, those options have disadvantages. Autograft caused morbidity of tissue to the patients. Allograft has the risk in the reduction of mechanical strength in the cryopreservation period. Xenograft has the risk of transgenic infections. Based on the problems mentioned, the development of synthetic ligaments has become a necessity.

Based on previous report, synthetic ligament from Poly Lactid Glicolic Acid (PLGA) was common [1]. PLGA sustained faster degradation than PLLA. It also sustained reduction of mechanical strength. The synthetic ligaments based on PTFE and Dacron sustained slower degradation time but it caused inflammation and foreign body reaction [1].

Freeman et al. (2006) conducted a research about in vivo test of the substitute ligament [2]. The materials were used were knitted PLLA, braided collagen and also braided PLLA. As the result, it was concluded that PLLA braided degradation time is the longest. It was around 48 weeks and the other materials degraded around 4 weeks-20 weeks. Freeman also conducted a research about the number of braid (yarn) for a scaffold. It was known that the number of braids that gave maximal

mechanical strength were around 2-4 braids. Synthetic ACL with two braids had ultimate tensile strength of  $71 \pm 7$  MPa, synthetic ACL with 4 braids had ultimate tensile strength of  $82 \pm 2$  MPa, while synthetic ACL with 6 braids had the lowest ultimate tensile strength of  $44 \pm 4$  MPa [2].

In this research, single braid was used because the objective in this study was to find out the influence of braiding angle variation to the tensile strength, not about the influence from the number of braids to the tensile strength. The second objective was to find out the influence of braiding angle to the size of pores because scaffold had the porosity requirements to enable bone and soft tissue growth. The third objective was to find the influence of braiding angle to the degradation rate of scaffold and the fourth objective was to prove that the material is nontoxic.

### Materials and Method

**Materials.** Poly L-lactid acid (PLLA) with  $M_w=180.000$  (Polysciotech) was used. Chloroform and toluene were of reagent grade (Merck). The equipments were electrospinning unit, stationary gap collector, magnetic stirrer, optical microscope, cytotoxicity kit, and simulated body fluid (SBF) kit.

**Fabrication of Scaffolds.** There were three processes to create the braided-twisted fiber scaffold. The first process was to create a homogenous solution. PLLA was dissolved in chloroform and toluene with concentration of 7% wt solute/wt solvents. The comparison of chloroform and toluene were 3:1. The solution was stirred at 100-500rpm. The viscosity of the solution after stirred for 48 hours was 100dPa. After that, the solution was stored in the refrigerator for 24 hours. The second process was to create fibers by electrospinning. The setting was voltage of 9kV, flow rate of 36 mL/hour, distance between spinneret and collector was 4cm. Stationary gap collector was used with two parallel copper wires. One lap of electrospinning running was for 2x24 hours. After 2x24 hours, filaments of fibers were removed from between two parallel copper wires. Then it was cut into 2cm x 4cm for one filament (Fig. 1) and rolled to make it into rolled filament (Fig. 2). The third process was to twist and braid the filaments (Fig. 3). The twist process used  $60^\circ$  angles and was performed manually with some patterns. Twisting angle was counted based on horizontal axis. Three filaments were twisted each others to make one yarn. Then it was made 9 yarns. Then 3 yarns were braided each other to make a scaffold. First 3 yarns were braided with  $40^\circ$  angle, second 3 yarns were braided with  $60^\circ$  angle, and third 3 yarns were braided with  $80^\circ$  angle.



Fig. 1. Sheet filament



Fig. 2. Rolled filaments



Fig. 3. Single braided-twisted fibers

**Characterization.** First characterization was degradation test in simulated body fluid (SBF). The pH was used 7.4. The test was done for 67 hours. Second characterization was microstructure test used optical microscope. Third characterization was tensile test. The fourth characterization was cytotoxicity test using MTT- assay method. There were two equations that were used for analyze the result of characterization. In simulated body fluid test, the equation used was

$$\text{Degradation velocity (mpy)} = \frac{534 \cdot W}{D \cdot A \cdot T} \quad (1)$$

with  $W$  is weight loss (mg),  $D$  is density ( $\text{g/cm}^3$ ),  $A$  is exposed extent ( $\text{cm}^2$ ), and  $T$  is exposure time (hours).

For MTT- assay test, the equation used was

$$\text{Percentage of livingcell} = \frac{OD_{\text{sample}} + OD_{\text{MediaControl}}}{OD_{\text{Cell}} + OD_{\text{MediaControl}}} \quad (2)$$

### Results and Discussion

The result of degradation test is shown in Table 1. The degradation was 2% for 40° sample, 3.6% for 60° sample, and 14.8% for 80° sample. Then it was counted time for the scaffold to discharge completely. For sample with 40° angle, the initial weight was 0.123 gram. The weight loss was 6.4 mg every 67 hours. It can be concluded that the scaffold will be completely discharged for 1287 hours or around 53 days. Based on the previous study that was conducted by Gulotta and Rodeo (2007), it was mentioned that perfect regeneration of bone and soft tissue were around 8-12 weeks. The braided-twisted fiber scaffold in this research was suitable with the minimum standard. For reducing the degradation velocity, it can be done by adding more braids in the scaffold [3].

Table 1. Degradation test in Simulated Body Fluid

Braiding angle	Exposed extent [in <sup>2</sup> ]	Ekspose time [hours]	Weight loss [mg]	Degradation velocity [mpy]
40°	0.0452	67	6.4	0.903
60°	0.0804	67	11.4	0.905
80°	0.1256	67	18.3	0.930

Range of pore sizes was measured by pore counting with microscope tile. From Table 2, it can be concluded that larger braiding angle gave larger pore size. Based on another preliminary study conducted by Yahia (1997), it was reported that pore size to sustain bone into the scaffold growth was 150 μm and the pore size to sustain soft tissue into the scaffold growth was 200 μm-250 μm [4]. Based on this, the sample with 40° braiding angle was not an ideal scaffold for bone and soft tissue growth. The sample with 60° can sustain bone growth, but it was not for the soft tissue. The sample with 80° scaffold was an ideal scaffold.

Table 2. Braiding angle variation related to the pore size of scaffold

Braiding angle	Range of pore size [μm]
40°	105-126
60°	127-170
80°	199-321

From tensile test (Table 3), it could be concluded that larger braiding angle gave lower tensile strength. The tensile strength of human ACL is 38±9 MPa. It must be noticed that in this experiment the number of braids was just a single braid while human ACL is multilayered. For increasing the tensile strength, the number of braids can be added. Because the thickness of filament layer which was cut between two wires was not uniform, the roll filaments were classified into three classes. First was low weight class of between 0.0042 gram and 0.0193 gram. Second was medium weight class of 0.0194 - 0.0386 gram. Third was high weight class between 0.0387 and 0.0537 gram. Then the filaments were grouped as their own classes. The purpose of this classification was to make uniform filaments in each scaffold because differences of filaments in a scaffold can be a trigger of fracture.

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Table 3. The influence of braiding angle variation to the tensile strength of scaffold

Parameter	Angle variation of braided-twisted fiber scaffold		
	40°	60°	80°
Tensile strength	1,318 MPa	0,22 MPa	0,024 MPa

Table 4. Optical density value for cytotoxicity test with MTT-Assay

Parameter	Optical density (OD) value
Media control	0.0702
Cell control	0.2607
Sample *	0.2197

A random sample was used for cytotoxicity test without repetition because the braiding angle variation is a physical variation; it should not influence the chemical condition of the scaffold. The result in Table 4 was substituted into the equation 2, and the result was 86.1%. From previous study, it has been known that a material is toxic if the value of optical density was less than 60% [5]. From this result, it can be concluded the braided-twisted fiber scaffold was nontoxic materials. It was a nontoxic material because the toxic solvents such chloroform and toluene has been evaporated perfectly during the process of electrospinning. This phenomena was caused by the use of high voltage. Bigger braiding angle of braided twisted fiber scaffold has high degradation rate, bigger pore size, and lower mechanical strength. The braided-twisted fiber scaffold was a nontoxic material due to percentage of living cell of more than 60%. The best braiding angle if reviewed from standard of pore size and cytotoxicity is 80°. The mechanical performance and the degradation rate can be repaired by adding braids in the scaffold. The best braiding angle with highlight in pore size related to capability of cell to be growth and its cytotoxicity level captured from the percentage of living cell is 80°. The optimalization of mechanical performance and the degradation rate might be repaired by adding the number of braided in the scaffold.

### Acknowledgement

This paper is performed by the funding from Directorate of Higher Education (DIKTI). This investigation and the paper were supported in part, national nuclear agency for electrospinning unit, and also Mr. Ali Akbar and Mr. Jan Setiawan for the support and advice in this research.

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10.4028/www.scientific.net/AMR.845

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10.4028/www.scientific.net/AMR.845.925

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10.1007/978-3-642-60428-7

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